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(54) Improved occluder for repair of cardiac and vascular defects

Okklusionsvorrichtung zur Reparatur von Herz- und Gefäss-Defekten

Dispositif d'occlusion, destiné à la réparation des défauts du coeur et des vaisseaux sanguins

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Description

The present invention relates to devices for the repair of intracardiac and vascular septal defects by percutaneous catheter placement of a corrective prosthetic device.

Either congenitally or by acquisition, abnormal openings or holes can occur between adjacent chambers of the heart or its associated major blood vessels. Such openings are referred to, respectively, as interatrial and interventricular septal defects or patent ductus arteriosus and cortico-pulmonary windows. Such openings cause blood to leak from one chamber or artery to another and result in decreased pumping efficiency of the heart. Similarly, if defects occur in the Foramen Ovale, such defects, referred to as Patent Foramen Ovale (PFO), may result in a cerebral embolism. These deformities usually are congenital; however, they can also occur following a heart attack, significantly complicating subsequent coronary treatment and recovery. Such defects typically impose added strain on the heart and ultimately may lead to heart failure if not corrected.

Traditionally, such defects have required extensive open chest surgical techniques for correction. Specifically, the repair of such defects required an open heart procedure in which the heart was exposed and then opened and the defect was sewn shut by direct suturing. In connection therewith, a patch of a synthetic prosthetic material such as Dacron, Teflon, silk, nylon or pericardium was used to repair the defect (Dacron and Teflon are registered Trade Marks).

Although other methods of occluding defects, most notably the use of a plastic plug to occlude the defect, were suggested as early as the 1950s, such methods similarly require the use of open heart surgery to access the defect and place the prosthetic implant.

Beginning in the early 1970s, a number of devices and methods were proposed for the percutaneous transluminal catheterization procedure for the repair of intracardiac defects. For example, U.S. Patent No. 3,874,388 to King et al., describes a device in which a pair of umbrella-like occluders are positioned on opposite sides of a defect and drawn and locked together at a central hub which crosses the defect. The device is said to effectively occlude the defect. Although the King device and method proposed to eliminate the need to perform open heart surgery, its use and structure were very complicated in that generally they required the umbrella-like occluders to be opened manually once positioned at the defect.

Similarly, U.S. Patent No. 4,007,743 to Blake relates to an umbrella-like defect closure device having a plurality of elongated struts pivotally mounted to a central hub. Each pair of adjacent struts is interconnected by a strip formed of a foldable, resilient material which serves to automatically and resiliently open each umbrella-like element once such element is released from a protective sheath. As in the King patent, the device includes two separate occluders which are locked together by a snap connection once each of the occluder segments has been individually positioned across the septal defect.

Still another defect closure device is described in U.S. Patent No. 4,917,089 to Sideris. The Sideris patent relates to an apparatus and method for transvenous closure of a septal perforation in the heart. The closure apparatus comprises an occluder which is positioned on the distal side of the perforation and an occluder-holder which is positioned on the proximal side of the perforation and is connected to the occluder across the perforation by means of a so-called "button" closure. As in the earlier transluminally delivered occluders, the Sideris patent requires that device elements positioned on opposite sides of a septal defect are separately delivered to the site of the defect and connected to one another in situ.

In EP-A-545091, filed concurrently herewith, and entitled "Occluder and Method for Repair of Cardiac and Vascular Defects" attempts to overcome problems associated with the aforementioned devices are described. The application describes a device having separate occlusion elements that are connected in a manner such that they may be oriented in aligned or nonaligned relationships across the defect. Such a device is particularly useful in the repair of tunnel-like defects or defects having a non-uniform wall thickness. The application also describes a device having occlusion elements that are fluoroscopically distinguishable from one another, thereby enhancing the ability of a physician to visualize the device fluoroscopically during a percutaneous, transluminal placement procedure.

The devices of the application described above typically comprise a series of elongated struts attached at a central point and having two flexural pivot points thereon. For example, in one embodiment, each elongated strut includes a first coil located on the strut at a position adjacent to a central portion of the device (referred to as a "shoulder" hinge), and a second coil located on the strut at a position remote from the shoulder (referred to as an "elbow" hinge). Despite the numerous advantages associated with the occluders described in the application above, on occasion such devices may fail as a result of stress or fatigue after a limited time in vivo. In particular, failures have occurred on the strut arm at the elbow hinge or at a region immediately adjacent thereto. Although such failures have resulted in no clinical problems (since the occluder rapidly becomes encapsulated in tissue prior to the incidence of failure), it would be desirable to eliminate even the possibility of such failures as a means of eliminating a potential source of complications.

Accordingly, a need exists for a device for the occlusion of cardiac and vascular defects that can withstand the full range of stresses applied to the device over a prolonged period of time in an in vivo environment. In connection therewith, a need exists for a vascular

occluder configured in a manner such that flexural stresses are minimized and distributed throughout the device in order to provide an occlusion device that will not undergo stress failures in vivo.

The present invention addresses the stress failure problem by providing struts which have at least three flexural points which serve to enhance resistance to failures caused by stress or fatigue. In particular, the invention relates to an intracardiac occlusion device that has been modified to reduce and/or more evenly distribute stresses that may arise in the device during movement of the heart. The resulting device has a structure having a resistance to fatigue exceeding the maximum fatigue stresses to which the device may be subjected during use.

Thus the present invention provides a device for percutaneous transluminal repair of septal defects comprising: a first occluder and a second occluder each having an initial cross sectional configuration smaller than that of a defect to be repaired and having a second expanded configuration larger than that of said defect; and a connector for fastening said first occluder to said second occluder; at least one of said first occluder or said second occluder including a framework comprising a central hub having a plurality of elongated struts radiating therefrom; characterised in that at least one of said struts includes three flexural points which provide the strut with a resistance to fatigue exceeding the maximum fatigue to which the strut may be subjected in vivo.

By selecting certain metallic alloy compositions for use in the device, the ability of the device to resist corrosion over an extended time in vivo can be additionally enhanced. This resistance to corrosion is believed to further enhance the device in its ability to resist failure over prolonged use.

Numerous modifications can assist in achieving the desired results, and combinations of two or more of such modifications can be used as well. Among the modifications useful for reducing stresses are the following:

a) substitution of wire having a square, rectangular, trapezoidal or triangular cross section for cylindrical wires that are currently used in occluder devices,
b) increasing the diameter of shoulder and elbow coils which constitute the flexural hinge points about which portions of the device may bend,
c) substituting an alloy comprising nickel, cobalt, chromium and molybdenum for the stainless steel alloys currently used to form the device, and
d) adding additional turns to coils constituting the flexural hinge points.

Additionally, when using the alloys described above the ultimate strength of the device can be further enhanced by annealing the framework of the device at a temperature of between about 232 and 538°C (450 and 1000°F) for several minutes. Such a process results in a precipitation hardening of the alloy, increasing both its strength and stiffness.

Thus with these modifications the design of the occluder device of the invention: provides increased resistance to stress failures and fatigue over a prolonged period of time;

reduces stresses that may occur in the device;
more evenly distributes stresses that may be contained in the device;
has inherent resistance to fatigue that may exceed the maximum fatigue stresses to which the device may be subjected over a prolonged period of time; and
resists corrosion over a prolonged in vivo exposure.

An embodiment of the occluder device of the invention will now be described by way of example and with reference to the accompanying drawings, in which:

FIG. 1 is a schematic illustration of one type of occluder device known to the prior art;
FIG. 2 is a schematic depiction of the cause of the stresses to which an occluder device can be subjected in vivo; and
FIG. 3 is a schematic illustration of one embodiment of an occluder device of the present invention.

Fig. 1 depicts an occlusion device of a type known in the prior art. As shown in Fig. 1, the device 10 comprises a first occluder 12 connected to a second occluder 14 in a face-to-face relationship. The occluders 12, 14 are connected to each other by means of a central hub or wire 16 which defines a central axis through each of the occluders 12, 14. It is noted that, as used herein, the term "central axis" is not meant to imply that the wire or hub is necessarily positioned at the geometric center, if any, of its respective occluder. Rather, the term is intended to describe a reference line oriented in a perpendicular relationship to the plane of each occluder, the line passing through any given reference point on the occluder.

Each occluder comprises generally a framework formed by a plurality of elongated struts 18 which radiate from the central hub 16 of the occluder. The framework can be collapsed and then automatically opened by resilient means which are provided in each of the elongated struts. Specifically, each strut includes at least one flexural hinge point or shoulder 20 about which the elongated strut 18 may flex. Such shoulders are positioned adjacent to the central hub of each occluder.

In a collapsed configuration, the elongated struts 18 are pivotally flexed about the shoulders 20 to cause the struts to be oriented in a position that is generally parallel to the central axis of the occluder defined by the hub or the wire 16. The struts are maintained in this position against resilient forces by enclosing the device within a

tubular sheath at the distal end of a delivery catheter which maintains the device in a collapsed configuration. Upon withdrawal of the sheath during the placement procedure, resilient forces stored within the elongated struts at the shoulders 20 cause the device to spring open by pivoting the struts about the hinge points defined by the shoulders. The struts 18 open to an orientation generally perpendicular to the central axis of the occluder.

The struts 18 include a second flexural hinge point or elbow 22 to provide a point on each strut about which the strut arm itself can fold, thereby allowing the length of the strut in its folded configuration to be shortened. In addition, the elbows serve as a location at which the struts may be preferentially bent in order to absorb stresses that may develop during movement of the septal wall in which the device is positioned as a result of the heart's natural rhythm.

Each strut preferably also includes a loop 24 at its distal end to conceal sharp areas that might otherwise damage tissue during insertion and placement of the device.

Attached to the strut frameworks are patches 26, 28 which, when the device is deployed, cover and occlude the shunt defect. Although numerous biocompatible materials can be used as the patch material, a material such as Dacron is typically used. Among the necessary characteristics of the patch material are biocompatibility and resistance to fluid transfer across the material. The material must be such that these properties can be maintained for extended periods in vivo. Additionally, the patch material must be flexible to allow the occluder device to be folded and compressed within a sheath prior to and during delivery to a predetermined location within a patient. An aperture 30 is formed within each of the patches 26, 28 and allows an interconnecting structure to connect the occluder elements to each other. The patches 26, 28 can be held to the strut framework by a plurality of stitches formed from sutures which encircle the struts and pass through the patch material.

Typically, occlusion devices of the above design employ 304V stainless steel wire having a circular cross-section and a diameter of approximately 0.25 mm (0.010 inches) to form the elongated struts or spring arms. In addition, each of the struts typically includes a shoulder 18 and an elbow 22, each of which comprises a coil having three turns. The inside diameter of the coils forming the shoulder hinge points is typically of the order of approximately 0.41 mm (0.016 inches), and the inside diameter of the coils forming the elbow hinge points is typically of the order of approximately 0.30 mm (0.012 inches).

An occluder of the type depicted in FIG. 1 is shown schematically as deployed across a septal defect in FIG. 2. It is noted that, as depicted in FIG. 2, when positioned in vivo, the occluders often have at least one strut that becomes displaced toward the center of the device as a result of contraction of the heart chamber. Specifically, a septum 40 having a defect comprising an aperture defined by walls 42 has an occlusion device 10 positioned therein. During pumping of the heart, portions 44 of the septum deflect as well (shown in phantom 44') causing the strut 18 in contact with the septal portion 44 to deflect (shown in phantom 18').

The deflection is believed to cause stresses that become manifested as metal fatigue in the elbows 22, thereby resulting in a stressed condition in such elbows 22'. Over repeated cycles of bending and releasing, as occurs by the natural pumping action of the heart, the metal that forms the elbow becomes fatigued and causes failures to develop in the device. These failures occur typically at the elbow 22 or on the strut arm 18 at a location immediately adjacent to the elbow.

One embodiment of an occlusion device having a reduced likelihood of metal fatigue failure at the elbow is depicted in Fig. 3. Such a device 50 comprises a pair of occluder elements 52, 54 connected to one another in a face-to-face relationship. The occluders 52, 54 are connected to each other by means of a central hub or wire 56 which defines a central axis through each of the occluders 52, 54. As in the device depicted in Fig. 1, the term "central axis" is intended only to describe a reference line oriented in a perpendicular relationship to the point of each occluder and passing through a given reference point on the occluder.

Each occluder includes a plurality of elongated struts 58 which radiate from the central hub and provide a framework for the occluder. As in the device described previously, the framework is adapted to be collapsed and then automatically opened by resilient means which are provided in each of the elongated struts 58. Specifically, each strut includes at least one flexural hinge point or shoulder 60 about which the elongated strut 58 may flex. In a collapsed configuration, the elongated struts 58 are pivotally flexed about the shoulders 60 to cause the struts to be oriented in a position that is generally parallel to the central axis of the occluder as defined by the hub or wire 56. The struts can be maintained in this position against resilient forces by enclosing the device with a tubular sheath located at the distal end of a delivery catheter which serves to maintain the device in a collapsed configuration. Upon withdrawal of the sheath during the placement procedure, resilient forces stored within the elongated struts at shoulders 60 cause the device to spring open resiliently by pivoting the struts about the shoulder. The struts 58 open to an orientation that is generally perpendicular to the central axis defined by the hub 56 of the occluder.

A second flexural hinge point or elbow 62 is provided on the strut 58 to further enhance operation of the occlusion device. As noted previously, the elbow provides a point about which the strut arm itself can fold, thereby allowing the length of the strut in its folded configuration to be shortened. Additionally, the elbows serve to absorb stresses which can be present within the framework of the device as a result of the natural

motion of the heart.

Each strut preferably also includes a loop 64 at its outer end to conceal sharp areas that might otherwise cause damage to tissue during insertion and placement of the device.

As in the device shown in FIG. 1, attached to the strut frameworks are patches 70, 72 which, when the device is deployed, cover and occlude the septal defect. Numerous biocompatible materials including Teflon, silk, nylon and pericardium can be used as the patch material; however, a material such as Dacron is preferred. Among the necessary characteristics of the patch material are biocompatibility and resistance to fluid transfer across the material. The material must be such that these properties can be maintained for extended periods in vivo. Additionally, the patch material must be flexible to allow the occluder device to be folded and compressed within a sheath prior to and during delivery to a predetermined location within a patient.

An aperture 74 is formed within each of the patches 70, 72 and allows an interconnecting structure to connect the occluder elements to each other. The patches 70, 72 can be held to the strut framework by a plurality of stitches formed from sutures which encircle the struts and pass through the patch material.

In a preferred embodiment, the stitches attach the patches to the framework at least at regions at which the shoulder and elbow hinge points 60, 62 and loops 64 contact the patch material. Alternatively, the sutures can be tied off at each loop and spiralled through the patch material and toward the central hub 56 terminating with knots tied to the hinge points. A ribbing 76 formed by a series of coarsely placed stitches is preferably formed along the peripheral edges of the patch material. The ribbing provides an area of increased patch material thickness and serves to provide a degree of stiffness and support to the outer edge of the patch material.

In the illustrative embodiment depicted in Fig. 3, each of the occluders 52, 54 is square. It is noted that the shape of the occluder elements is not intended to be limited as such. Rather, occluders having rectangular, circular or other geometries are contemplated as well and are intended to be encompassed within the scope of the invention.

Unlike the device depicted in Fig. 1, the device of Fig. 3 includes a third flexural hinge point or wrist 66 positioned on each strut 58 between the elbow 62 and the loop 64. The purpose of the wrist 66 is to reduce fatigue in the struts by absorbing and distributing stresses which can arise in the struts during natural movement of the heart. By providing an additional flexural point or coil in the form of a wrist 66 on each strut, the framework is provided with a means for distributing stresses more evenly, thereby reducing fatigue and significantly decreasing the possibility that failures can occur within the material forming the struts.

As noted previously, the present invention contemplates numerous ways by which stress and fatigue can be reduced in the occluder framework to effectively provide the device with infinite fatigue resistance. Thus, the device is expected to have a resistance to fatigue or stress failures which is greater than the maximum cumulative fatigue or stress to which the device will be subjected over the lifetime of the patient.

The specific modifications to the device for providing infinite fatigue and corrosion resistance include dimensional changes to the wire used to form the framework, changes to the diameter of the coils which comprise the shoulder and elbow of the framework, substitution of the metallic alloys used to form the framework structure, the addition of the third flexural hinge point (wrist) to the framework, variations in the number of turns in the flexural points, and any combination of the above improvements. Each of these is discussed separately below.

As discussed above, in the prior art the wire used to form the framework of the occluder elements was typically a wire having a circular cross section and a diameter of approximately 0.25 mm (0.01 inches). In connection with the present invention, however, it has been found that if a wire having a square, rectangular, trapezoidal or triangular cross section of approximately 0.13 to 0.38 mm (0.005-0.015 inches) on edge, is substituted for the round wires of the prior art devices, stresses within the device can be reduced. For example, in the case in which a square wire having a cross section of approximately 0.20 mm (0.008 inches) is used to form the occluder framework, stresses within the device can be reduced by approximately 29%. If a wire having a rectangular cross section is used, a wire of approximately 0.18 mm by approximately 0.23 mm (0.007 inches by 0.009 inches) is preferred.

It should be noted, however, that it is not absolutely necessary that non-circular wire be used to form the device. Rather, wire having a circular cross section is contemplated as well. It is preferred that such a round wire have a diameter of approximately 0.23 mm (0.009 inches).

The devices of the prior art have flexural hinge points (the shoulder and elbow), which typically have been formed by wrapping the wire comprising the struts about mandrels. Typically, the mandrel used to form the shoulder coils has a diameter of approximately 0.41 mm (0.016 inches), while the mandrel used to form the elbow coils has a diameter of approximately 0.30 mm (0.012 inches). In connection with the invention, it has been found that if a mandrel having a diameter of approximately 0.25 to 0.64 mm (0.010-0.025 inches) is used to form both the shoulder and the elbow coils which form the flexural hinge points, stresses in the device can be reduced. In particular, if a mandrel having a diameter of approximately 0.41 mm (0.016 inches) is used to form the flexural hinge points, stresses in the occluder framework can be reduced by approximately 22%.

The material that has been used to form the framework for the occluders of the prior art was typically 304V stainless steel. In connection with the present invention, a metallic alloy such as MP35N available from Maryland Specialty Wire, Inc. (Cockeysville, Maryland 21030, USA) or a metallic alloy such as Elgiloy® available from Elgiloy Company (Elgin, Illinois 60123, USA) has been substituted. The substitution of these particular alloys for the 304V wire of the prior art has been found to provide the occluder with an increased stress capability of approximately 14%. In addition, the substitution of the above metallic alloys for the 304V stainless steel of the prior art has been found to provide enhanced resistance to corrosion to the occluders of the present invention. The reduction or elimination of corrosion is believed to further decrease the possibility of device failure during prolonged exposure to an in vivo environment.

MP35N is a metallic alloy composition comprising approximately 35% nickel, 35% cobalt, 20% chromium, and approximately 9.75% molybdenum. The alloy is a multiphase alloy that is face-centered-cubic (fcc) in the annealed condition and has a microstructure similar to that of austenitic stainless steel. When the alloy is cold-worked, such as when it is drawn to form a wire, the microstructure changes so that a portion of the fcc phase transforms to a hexagonal close-packed phase. This phase transformation results in an increase in the strength of the wire. A suitable degree of phase transformation is believed to occur for wires that have been cold-worked by drawing to result in a 30-80% reduction in cross-sectional area.

Additional strengthening of the wire can be obtained when a cold-worked structure, such as a drawn wire formed into an occluder framework, is subjected to an ageing treatment at an elevated temperature. In connection therewith, heating the alloy for several minutes at a temperature in the range of approximately 232 to 538°C (450°-1000°F) causes a precipitation hardening of the alloy which increases both its strength and its stiffness.

Similarly, Elgiloy is a metallic alloy composition comprising 39-41% cobalt, 19-21% chromium, 14-16% nickel, 6-8% molybdenum, 1.5-2.5% manganese, 0-0.15% carbon, 0-0.1% beryllium and the balance comprising iron. Like MP35N, Elgiloy is preferred for use in the present invention due to its strength, stiffness, and resistance to structural failure under the conditions at which the occluder device is expected to be used.

Still another change is the addition of an extra spring coil (the wrist coil 66) as shown in Fig. 3. The use of a wrist coil 66 has been found to reduce stresses in the device by approximately 50% as a result of complimentary load sharing between the wrist, elbow and shoulder flexural points. It is preferred that the wrist coil have two turns and be formed on a mandrel having a diameter of approximately 0.25 to 0.64 mm (0.010-0.025 inches). In this range, a diameter of approximately 0.41 mm (0.016 inches) is most preferred.

Finally, in some circumstances, it has been found desirable to vary the number of turns of the coils comprising the flexural points. For example, when each of the flexural hinge points comprises a coil having three turns, stresses in the wire framework have been found to decrease by approximately 50%.

In one preferred embodiment, the occlusion device includes two occluders each of which are formed of MP35N alloy in the form of 0.20 mm (0.008 inch) square wire. The wire is used to form an occluder framework having four struts, each of said struts including flexural hinge points defining a shoulder, an elbow and a wrist as well as a loop on the distal end of each strut. It is preferred that the shoulder and wrist hinge points be formed of coils each having two turns of wire and the elbow hinge point be formed of a coil having three turns of wire. The inside diameter of at least the wrist and shoulder coils are preferably about 0.41 mm (0.016 inches). The inside diameter of the elbow coil may also be about 0.41 mm (0.016 inches) or, in the alternative, it can have a slightly smaller diameter of approximately 0.30 mm (0.012 inches). As noted previously, once formed, the framework can be heated to a temperature of between approximately 232 and 538°C (450° and 1000°F) for a period of time sufficient to cause precipitation hardening of the alloy forming the framework, thereby enhancing the strength and stiffness of the occluder.

Claims

1. A device (50) for percutaneous transluminal repair of septal defects comprising:

   a first occluder (52) and a second occluder (54) each having an initial cross sectional configuration smaller than that of a defect to be repaired and having a second expanded configuration larger than that of said defect; and
   a connector (56) for fastening said first occluder to said second occluder;
   at least one of said first occluder or said second occluder including a framework comprising a central hub (56) having a plurality of elongated struts (58) radiating therefrom;
   characterised in that at least one of said struts includes three flexural points (60,62,66) which provide the strut with a resistance to fatigue exceeding the maximum fatigue to which the strut may be subjected in vivo.

2. The device of claim 1 wherein said at least one elongated strut comprises a wire having a square, rectangular, trapezoidal or triangular cross section.

3. The device of claim 2 wherein said cross section is approximately 0.13 to 0.38 mm on edge.

4. The device of claim 2 wherein said at least one elongated strut comprises a wire having a square cross section of approximately 0.20 mm on edge.

5. The device of claim 2 wherein said at least one elongated strut comprises a wire having a rectangular cross section of approximately 0.18 mm by approximately 0.23 mm.

6. The device of claim 1 wherein said at least one elongated strut comprises a wire having a round cross-section.

7. The device of claim 6 wherein said at least one elongated strut comprises a wire having a round cross section of approximately 0.23 mm in diameter.

8. The device of claim 1 wherein said flexural hinge points (60,62,66) comprise coiled portions of the elongated strut (58).

9. The device of claim 8 wherein said coiled portions have an inner diameter of approximately 0.25 to 0.64 mm.

10. The device of claim 8 wherein said coiled portions have an inner diameter of approximately 0.41 mm.

11. The device of claim 8 wherein said coiled portions include at least two coils.

12. The device of claim 8 wherein said coiled portions include at least three coils.

13. The device of claim 1 wherein said at least one elongated strut (58) comprises a wire fabricated of a metallic alloy containing nickel, cobalt, chromium and molybdenum.

14. The device of claim 13 wherein said alloy comprises approximately 35% nickel, 35% cobalt, 20% chromium and 9.75% molybdenum.

15. The device of claim 14 wherein said alloy further comprises manganese, carbon, beryllium and iron.

16. The device of claim 14 wherein said alloy comprises at least approximately 14% nickel, 39% cobalt, 19% chromium, 6% molybdenum and 1.5% manganese.

17. The device of claim 15 wherein said alloy further comprises up to approximately 0.15% carbon and 0.1% beryllium.

18. The device of claim 15 wherein said alloy further comprises iron.

19. The device of claim 13 wherein said alloy is annealed to a degree sufficient to cause precipitation hardening thereof.

20. The device of claim 13 wherein said wire has been cold-worked to reduce its cross-sectional area by approximately 30 to 80%.

21. The device of claim 19 wherein said annealing is carried out at a temperature between 232 and 538°C.

22. The device of claim 1 wherein said framework is fabricated of a wire having a square, rectangular, round, trapezoidal or triangular cross section and having a metallic alloy composition comprising nickel, cobalt, chromium and molybdenum,
and wherein each of said elongated struts (58) includes three flexural hinge points (60,62,66).

23. The device of claim 22 wherein said metallic alloy composition is annealed to a degree sufficient to cause precipitation hardening thereof.

24. The device of claim 22 wherein said metallic alloy composition comprises approximately 35% nickel, 35% cobalt, 20% chromium and 9.75% molybdenum.

25. The device of claim 22 wherein said metallic alloy composition comprises 39-41% cobalt, 19-21% chromium, 14-16% nickel, 6-8% molybdenum, 1.5-2.5% manganese, 0 to 0.15% carbon, 0 to 0.1% beryllium and the balance of iron.

26. The device of claim 22 wherein said flexural hinge points (60,62,66) comprise coiled portions of the elongated strut (58).

Patentansprüche

1. Vorrichtung (50) zur perkutanen transluminalen Reparatur von Septumdefekten, mit:

einem ersten Verschlußmittel (52) und einem zweiten Verschlußmittel (54), wobei jedes eine ursprüngliche Querschnittskonfiguration, die kleiner als diejenige des zu reparierenden Defektes ist, und eine zweite expandierte Konfiguration, die größer als diejenige des Defektes ist, aufweist; und
einem Verbindungsmittel (56) zum Befestigen des ersten Verschlußmittels an dem zweiten Verschlußmittel;
wobei wenigstens eines der ersten und zweiten Verschlußmittel einen Tragerahmen mit einer zentralen Nabe (56) umfaßt, die mehrere, von ihr radial wegführende, ausgedehnte Streben

(58) aufweist;

dadurch gekennzeichnet, daß wenigstens eine der Streben drei Biegestellen (60,62,66) umfaßt, die der Strebe eine Ermüdungsbeständigkeit verleihen, welche die maximale Ermüdung übertrifft, welcher die Strebe in-vivo ausgesetzt sein kann.

2. Vorrichtung gemäß Anspruch 1, wobei die wenigstens eine ausgedehnte Strebe einen Draht mit einem quadratischen, rechteckigen, trapezförmigen oder dreieckigen Querschnitt umfaßt.

3. Vorrichtung gemäß Anspruch 2, wobei der Querschnitt eine ungefähre Kantenlänge von 0,13 bis 0,38 mm aufweist.

4. Vorrichtung gemäß Anspruch 2, wobei die wenigstens eine ausgedehnte Strebe einen Draht umfaßt, der einen quadratischen Querschnitt mit etwa 0,20 mm Kantenlänge aufweist.

5. Vorrichtung gemäß Anspruch 2, wobei die wenigstens eine ausdehnte Strebe einen Draht umfaßt, der einen rechteckigen Querschnitt von etwa 0,18 mm auf etwa 0,23 mm Kantenlänge aufweist.

6. Vorrichtung gemäß Anspruch 1, wobei die wenigstens eine ausdehnte Strebe einen Draht mit rundem Querschnitt umfaßt.

7. Vorrichtung gemäß Anspruch 6, wobei die wenigstens eine ausdehnte Strebe einen Draht umfaßt, der einen runden Querschnitt mit etwa 0,23 mm Durchmesser aufweist.

8. Vorrichtung gemäß Anspruch 1, wobei die scharnierartigen Biegestellen (60,62,66) gewickelte Abschnitte der ausgedehnten Strebe (58) umfassen.

9. Vorrichtung gemäß Anspruch 8, wobei die gewikkelten Abschnitte einen Innendurchmesser von etwa 0,25 bis 0,64 mm aufweisen.

10. Vorrichtung gemäß Anspruch 8, wobei die gewikkelten Abschnitte einen Innendurchmesser von ungefähr 0,41 mm aufweisen.

11. Vorrichtung gemäß Anspruch 8, wobei die gewikkelten Abschnitte wenigstens zwei Wicklungen umfassen.

12. Vorrichtung gemäß Anspruch 8, wobei die gewikkelten Abschnitte wenigstens drei Wicklungen umfassen.

13. Vorrichtung gemäß Anspruch 1, wobei die wenigstens eine ausgedehnte Strebe (58) einen Draht umfaßt, der aus einer Metallegierung hergestellt ist, welche Nickel, Kobalt, Chrom und Molybdän enthält.

14. Vorrichtung gemäß Anspruch 13, wobei die Legierung etwa 35 % Nickel, 35 % Kobalt, 20 % Chrom und 9,75 % Molybdän umfaßt.

15. Vorrichtung gemäß Anspruch 14, wobei die Legierung außerdem Mangan, Kohlenstoff, Beryllium und Eisen umfaßt.

16. Vorrichtung gemäß Anspruch 14, wobei die Legierung wenigstens etwa 14 % Nickel, 39 % Kobalt, 19 % Chrom, 6 % Molybdän und 1,5 % Mangan umfaßt.

17. Vorrichtung gemäß Anspruch 15, wobei die Legierung außerdem bis zu etwa 0,15 % Kohlenstoff und 0,1 % Beryllium umfaßt.

18. Vorrichtung gemäß Anspruch 15, wobei die Legierung außerdem Eisen umfaßt.

19. Vorrichtung gemäß Anspruch 13, wobei die Legierung bis zu einem solchen Grad ausgeglüht ist, der ihre Ausscheidungshärtung bewirkt.

20. Vorrichtung gemäß Anspruch 13, wobei der Draht kaltverformt wurde, um seine Querschnittsfläche um etwa 30 bis 80 % zu reduzieren.

21. Vorrichtung gemäß Anspruch 19, wobei das Ausglühen bei einer Temperatur zwischen 232 und 538 °C durchgeführt wird.

22. Vorrichtung gemäß Anspruch 1, wobei der Tragerahmen aus einem Draht hergestellt ist, der einen quadratischen, rechteckigen, runden, trapezförmigen oder dreieckigen Querschnitt und eine Metallegierungszusammensetzung aufweist, die Nickel, Kobalt, Chrom und Molybdän umfaßt

und wobei jede der ausgehnten Streben (58) drei scharnierartige Biegestellen (60,62,66) umfaßt.

23. Vorrichtung gemäß Anspruch 22, wobei die Metallegierungszusammensetzung bis zu einem solchen Grad ausgeglüht ist, der ihre Ausscheidungshärtung bewirkt.

24. Vorrichtung gemäß Anspruch 22, wobei die Metallegierungszusammensetzung etwa 35 % Nickel, 35 % Kobalz, 20 % Chrom und 9,75 % Molybdän umfaßt.

25. Vorrichtung gemäß Anspruch 22, wobei die Metall-

legierungszusammensetzung 39-41 % Kobalt, 19-21 % Chrom, 14-16 % Nickel, 6-8 % Molybdän, 1,5-2,5 % Mangan, 0 bis 0,15 % Kohlenstoff, 0 bis 0,1 % Beryllium und der Rest Eisen umfaßt.

26. Vorrichtung gemäß Anspruch 22, wobei die scharnierartigen Biegestellen (60,62,66) gewickelte Abschnitte der ausgedehnten Strebe (58) umfassen.

Revendications

1. Dispositif (50) pour intervention réparatrice transluminale percutanée de déficiences septales comprenant :

   un premier dispositif d'occlusion (52) et un deuxième dispositif d'occlusion (54) ayant chacun une conformation initiale de section transversale plus petite que celle d'une déficience à réparer et ayant une deuxième conformation dilatée plus grande que celle de ladite déficience; et
   un connecteur (56) pour solidariser ledit premier dispositif d'occlusion audit deuxième dispositif d'occlusion ;
   au moins l'un dudit premier dispositif d'occlusion ou dudit deuxième dispositif d'occlusion comportant une ossature comprenant un moyeu central (56) ayant plusieurs entretoises allongées (58) rayonnant à partir de lui ;
   caractérisé en ce que au moins l'une desdites entretoises comporte trois points de flexion (60, 62, 66) qui procurent à l'entretoise une résistance à la fatigue dépassant la fatigue maximale à laquelle l'entretoise peut être soumise in vivo.

2. Dispositif selon la revendication 1 dans lequel ladite au moins une entretoise allongée comprend un fil ayant une section transversale carrée, rectangulaire, trapézoïdale ou triangulaire.

3. Dispositif selon la revendication 2 dans lequel ladite section transversale a approximativement 0,13 à 0,38 mm de côté.

4. Dispositif selon la revendication 2 dans lequel au moins une une entretoise allongée comprend un fil ayant une section transversale carrée d'approximativement 0,20 mm de côté.

5. Dispositif selon la revendication 2 dans lequel ladite au moins une entretoise allongée comprend un fil ayant une section transversale rectangulaire d'approximativement 0,18 mm x 0,23 mm.

6. Dispositif selon la revendication 1 dans lequel au moins une une entretoise allongée comprend un fil ayant une section transversale circulaire.

7. Dispositif selon la revendication 6 dans lequel au moins une entretoise allongée comprend un fil ayant une section transversale circulaire d'approximativement 0,23 mm de diamètre.

8. Dispositif selon la revendication 1 dans lequel lesdits points d'articulation de flexion (60, 62, 66) comprennent des parties enroulées de l'entretoise allongée (58).

9. Dispositif selon la revendication 8 dans lequel lesdites parties enroulées ont un diamètre intérieur d'approximativement 0,25 à 0,64 mm.

10. Dispositif selon la revendication 8 dans lequel lesdites parties enroulées ont un diamètre intérieur d'approximativement 0,41 mm.

11. Dispositif selon la revendication 8 dans lequel lesdites parties enroulées comportent au moins deux enroulements.

12. Dispositif selon la revendication 8 dans lequel lesdites parties enroulées comportent au moins trois enroulements.

13. Dispositif selon la revendication 1 dans lequel ladite au moins une entretoise allongée (58) comprend un fil fabriqué en un alliage métallique contenant du nickel, du cobalt, du chrome et du molybdène.

14. Dispositif selon la revendication 13 dans lequel ledit alliage comprend approximativement 35 % de nickel, 35 % de cobalt, 20 % de chrome et 9,75 % de molybdène.

15. Dispositif selon la revendication 14 dans lequel ledit alliage comprend de plus du manganèse, du carbone, du béryllium et du fer.

16. Dispositif selon la revendication 14 dans lequel ledit alliage comprend au moins approximativement 14 % de nickel, 39 % de cobalt, 19 % de chrome, 6% de molybdène et 1,5 % de manganèse.

17. Dispositif selon la revendication 15 dans lequel ledit alliage comprend de plus jusqu'à approximativement 0,15 % de carbone et 0,1 % de béryllium.

18. Dispositif selon la revendication 15 dans lequel ledit alliage comprend de plus du fer.

19. Dispositif selon la revendication 13 dans lequel ledit alliage est recuit à un niveau suffisant pour provoquer un durcissement par précipitation de celui-ci.

20. Dispositif selon la revendication 13 dans lequel ledit fil a été écroui à froid pour réduire la surface de sa section transversale d'environ 30 à 80 %.

21. Dispositif selon la revendication 19 dans lequel ledit recuit est accompli à une température entre 232 et 538° C.

22. Dispositif selon la revendication 1 dans lequel ladite ossature est fabriquée en un fil ayant une section transversale carrée, rectangulaire, circulaire, trapézoïdale ou triangulaire et ayant une composition d'alliage métallique comprenant du nickel, du cobalt, du chrome et du molybdène,
et dans lequel chacune desdites entretoises allongées (58) comporte trois points d'articulation de flexion (60, 62, 66).

23. Dispositif selon la revendication 22 dans lequel ladite composition d'alliage métallique est recuite à un niveau suffisant pour provoquer un durcissement par précipitation de celle-ci.

24. Dispositif selon la revendication 22 dans lequel ladite composition d'alliage métallique comprend approximativement 35 % de nickel, 35 % de cobalt, 20 % de chrome et 9,75 % de molybdène.

25. Dispositif selon la revendication 22 dans lequel ladite composition d'alliage métallique comprend 39 à 41 % de cobalt, 19 à 21 % de chrome, 14 à 16 % de nickel, 6 à 8 % de molybdène, 1,5 à 2,5 % de manganèse, 0 à 0,15 % de carbone, 0 à 0,1 % de béryllium, et le complément de fer.

26. Dispositif selon la revendication 22 dans lequel lesdits points d'articulation de flexion (60, 62, 66) comprennent des parties enroulées de l'entretoise allongée (58).

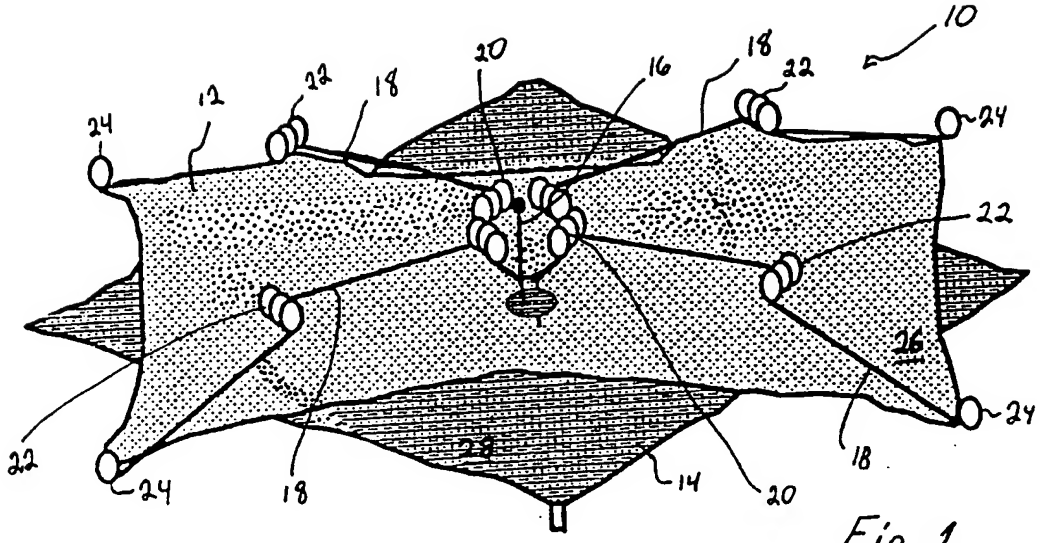

Fig. 1

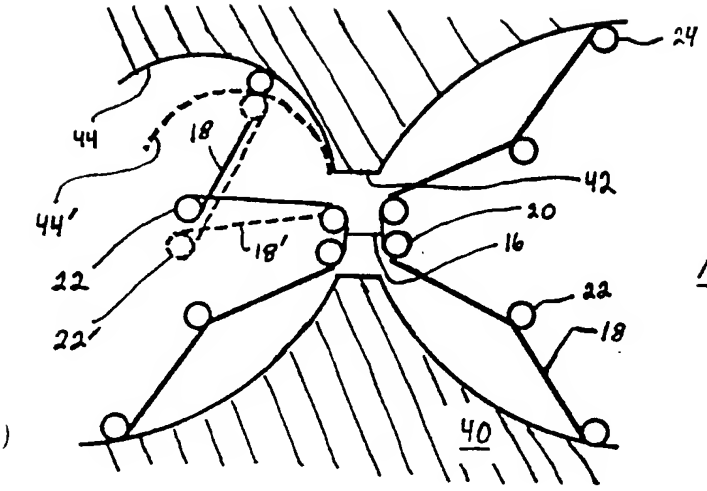

Fig. 2

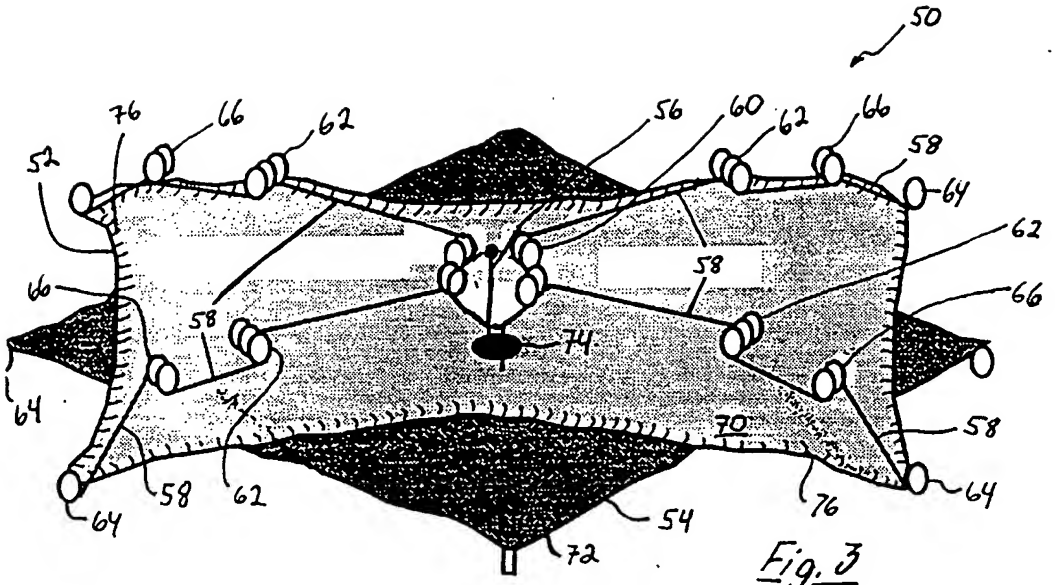
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Fig. 3